

Shear Stress Biology of the Endothelium

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Abstract—The relationships between blood flow, mechanotransduction, and the localization of arterial lesions can now be advanced by the incorporation of new technologies and the refinement of existing methods in imaging modalities, computational modeling, fluid dynamics, and high throughput genomics and proteomics. When combined with traditional cell and molecular technologies, a powerful palette of investigative approaches is available to address shear stress biology of the endothelium at levels extending from nanoscale subcellular detailed mechanistic responses through to higher organizational levels of regional endothelial phenotypes and heterogeneous vascular beds.

Keywords—Mechanotransduction, Biomechanics, High throughput analyses, Atherosclerosis, Vascular biology

INTRODUCTION

The vessel wall reacts to multiple chemical and mechanical stimuli in the flowing blood; the mechanical factors are principally pressure and shear stress. These responses often function in a feedback manner either to control blood flow or adapt the vessel structure to its required function.^{7,19,54} The general health of the vessel wall is dependent on the shear that it experiences via the endothelial interface and the resulting mechanosensing mechanisms of the endothelial cells.⁹ This position paper is focused on the blood flow–vessel wall interactions related to shear.

Interest in shear stress biology of the endothelium is principally directed to three related objectives: (i) understanding the function of shear in integrated vascular physiology, particularly in resistance vessels and arterial remodeling, (ii) a detailed understanding of the cellular mechanisms by which shear stress influences endothelial biology at multiple levels, mostly physiological, and (iii) an understanding of the relationships between hemodynamic forces and the localization of atherosclerosis, a disorder in which the endothelium plays a critical pathogenic role.

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SHEAR STRESS AND PHYSIOLOGICAL RESPONSES

That increasing blood flow through arteries results in vasodilation was first observed in larger arteries in 1933.⁴⁷ However, it was more than 50 years later that the role of the endothelium in this response was established by varying the viscosity of perfusion medium in isolated artery preparations thereby demonstrating that shear stress was an important factor.^{29,31,41} The isolated perfused resistance artery preparation became important in quantifying these acute responses as a function of vessel diameter and its interaction with spontaneous or induced myogenic tone.³⁴ It is thought that shear-induced mediation is important in organ flow control since it amplifies the dilatory stimulus of the smallest arterioles due to the larger more proximal ones.⁷ Furthermore, wall shear stress has been implicated in the development and adaptation of vascular beds,^{30,38} and in the chronic physiological remodeling of large arteries²⁰ where the presence of the endothelium determines the outcome.³⁵ Although theoretical and experimental studies^{1,43} implicate shear as only one of the determinants of vascular adaptation,^{23,44} the endothelium clearly plays a central role, and its relationship to shear stress needs to be understood.

SHEAR STRESS ENDOTHELIAL MECHANOTRANSDUCTION

The investigation of shear stress relationships to the endothelium *in vitro* is now a mature field that began shortly after the successful sustained culture of differentiated endothelial cells when flow devices used in fluid dynamics research were seeded with an endothelial lining.¹⁵ Easy access to the cells and ready manipulation of the flow characteristics provided descriptions of morphological and cytoskeletal changes and the development of simple computational analyses of the changes,^{36,45} calculations of flow characteristics and shear stresses were based on classical fluid dynamics. Subsequently, the averaged cellular responses of monolayers of cultured cells were measured^{10,11,48} which led to the detailed probing of single living cells^{14,26,39} including computational measurements

using sophisticated techniques, e.g. surface topography, cytoskeletal protein dynamics, and more recently an appreciation of the potentially important role of the luminal glycocalyx, a carbohydrate-rich surface coat consisting of the ectodomains of glycoproteins and proteoglycans.^{6,50,56} Better definition of the actual sites of initial interactions between shear and the cell has extended the force–cell relationship beyond the surface structures into the interior of the cell. This has led to an improved understanding of mechanotransmission throughout the cytoskeleton and the development of intracellular strain maps.²⁵ From spatial images of adhesion sites, junctions, and cytoskeletal dynamics a decentralized view of mechanotransduction has evolved⁴ that has been confirmed by sophisticated molecular probing of discrete subcellular locations (e.g., Ref. 49). However, spatial mapping of cellular biomechanics and the temporal relationships remain poorly understood. Advances in cell and molecular imaging, metabolic markers and other probes, provide great opportunities to correct this deficit.

SHEAR STRESS ENDOTHELIAL BIOLOGY AND ATHEROSCLEROSIS

It is a longstanding observation that atherosclerosis is not evenly distributed over the arterial system. A few decades ago both high and low shear stress were postulated as an explanation for this uneven distribution of atherosclerosis^{4,16,17} coincidental with the unequivocal demonstration of the retention of endothelium during atherogenesis,¹³ a finding that first implicated endothelial functional phenotype as a critical factor in the shift from normal physiology to flow-directed focal pathology. Since then, evidence supporting average low shear stress as a plaque-modulating factor^{21,32,33,53,55,58} has accumulated although the complex flow characteristics in these regions may be as important as the average magnitude of the stress *per se*.¹⁰ Based upon these observations, several rheological theories have been postulated, including dispersion of LDL particles towards the vessel wall,⁵⁷ shear-dependent accumulation of inflammatory cells^{27,28} and shear stress dependent gene expression of the endothelial cell.^{22,37,46} The last theory is receiving attention with focused efforts to dissect cellular biomechanical mechanisms during the past decade (briefly noted above) have been assisted by developments in molecular genetics that permit localized endothelial analyses (vascular bed and regional profiles) to be addressed. Developments include the functional analysis of the consequences of genetic manipulation in intact mammals through gene knock-out and transgenic methods,^{8,51} the measurement of candidate genes *in situ*,^{14,24} the development of high throughput arrays that facilitate profiling of endothelial phenotypes *in vitro*,^{3,5,18,52} and recently, phenotype profiles in highly localized regions of arteries *in vivo*,⁴⁰ the latter following refinements of RNA amplification methods to improve the fidelity of differential

gene expression.⁴² These approaches are suited to detailed ‘global’ investigations of detailed pathways of shear stress transmission and mechanotransduction in the endothelial cell and the important mapping of endothelial biology and pathology in relation to atherogenesis. However, it is essential that well-designed statistics and bioinformatics are used in microarray studies in accordance with fast-developing international standards.² There are now great opportunities to apply a range of length scales to investigate shear stress endothelial mechanotransduction leading to convergence¹² of the regional behaviour of endothelium *in vivo* with the detailed cellular and molecular responses in single living cells in real time at nanoscale resolution.

FUTURE DIRECTIONS

Present and future approaches are limited only by the imagination of the investigator; however, from a careful review of the literature we propose several broad priority objectives (not in any order):

- Adapt the latest technologies to the problem wherever possible by direct analyses of cells *in situ*, *in vivo*, or obtained immediately *post mortem*, i.e. retaining some characteristics of the *native vascular environment*.
- Design *in vitro* experiments that critically test the most dominant fluid dynamics characteristics that exist *in vivo* and test the conclusions by experiments *in vivo* or in intact tissues.
- Embrace the use of *high throughput genomics and proteomics* that simultaneously measure many variables from the same biological source to provide an integrated profile of cellular behavior. The technologies are applicable to smaller groups of cells and will eventually allow measurement of gene expression profiles of single endothelial cells *in vivo* and for cells *in vitro* for which computational and image-based information will be simultaneously gathered.
- Measure the local biomechanical environment at the *maximum resolution* appropriate to the system. Detailed knowledge of cellular geometry and structure is required. Approaches may include imaging of cell surface (e.g., AFM, TIRF), cytoskeleton (GFP and similar endogenous reporters), adhesion dynamics, subcellular localization of signaling molecules etc. Some of these measurements permit detailed, high resolution computation of localized stress concentrations (surface, cytoskeleton).
- Further develop cytomechanics in the *living* endothelial cell both *in vitro* and *in vivo*. Since structures ranging from the glycocalyx to the basal adhesion proteins are interconnected, *mechanotransmission* needs to be addressed by classical engineering to allow better interpretation of the biological responses, many of which are spatially accessible using molecular tags. This is an area where the biology is ahead of the mechanics.

- Prioritize *spatial and temporal relationships* when measuring force characteristics and cellular responses. The deformation of structural components needs to be measured as a function of time and space, and in relationship to the *timing* of biological signals. Confocal and deconvolution microscopy are particularly useful for 3-D and 4-D image reconstructions with z-resolution approaching 100 nm.
- Determine the importance of gradients of shear stress on endothelial biology and the temporal changes occurring throughout the cardiac cycle. All endothelium is subjected to cyclical shear stress. In most cases it is directional; in flow separation regions it is multidirectional, multi frequency, and momentarily zero. How does the cell filter these constantly changing stimuli?
- Incorporate *other biomechanical and cellular interactions* into the shear stress biology of the endothelium. A better understanding of non-shear components of vascular hemodynamics and their integration into current ‘dogmas’ would include other biophysical parameters of the blood vessel, e.g. diffusion and convective transport particularly in the glycocalyx, slip/non-slip conditions, the influence of hemodynamic pressure variables on smooth muscle cells communicating with the endothelium, etc.
- A detailed structural, dynamic, genetic, and functional analysis of the glycocalyx is required to better understand the initial contact of flowing plasma and the endothelial cell surface. Both mechanical deformation and transport characteristics are important considerations at this site.
- Investigate the shear stress biology of the endothelium in relation to *atherogenesis* over a range of length scales using both high throughput and single probe technologies, and with an emphasis on *in vivo* studies. Recent advances in nucleic acid amplification permit regional endothelial phenotyping *in vivo*, and single probe techniques for candidate gene expression provide high resolution spatial information *in situ*.
- Study other *important physiological and pathological mechanisms* in which shear stress is a factor, e.g. for the adhesion, rolling and arrest of immunocompetent cells at the endothelial surface; the expression of adhesion factors and force interactions between cells and proteins. Neovascularization is coupled to shear stress by angiogenesis and all shear stress related genes are now producing proteins from these vessels. Shear stress is strongly emerging as an important determinant of cardiac development.
- We recognize important links with the wider field of vascular biology, particularly in smaller arterial vessels. The stresses and strains of the intracellular skeleton induced by shear stress must bear a relation with those induced by other causes of cellular shape changes; for example during smooth muscle-regulated changes of vessel diameter, an event which also inevitably alters the shear

stresses. There is evidence that pressure as well as shear is a factor in vascular remodeling.

- Biofluid mechanics is undergoing recognition as an important component of many physiological and pathological processes and is therefore gaining interest and acceptance in many *biomedical and clinical* research areas. Most topically, they include cardiology (molecular and interventional), pathology, developmental biology, cell and molecular biology, and new avenues of interest in cancer biology and genetics. Biofluid dynamics will play a role in interventional cardiology as emerging techniques that enable the calculation of shear stress fields in relation to plaque characteristics in patients become available.

BIOFLUID MECHANICS AND THE NIH ROADMAP

The successful implementation of biofluid mechanics research requires the integrated efforts of investigators who usually have primary training in different disciplines and fields. There are many examples of successful collaborations between the biophysical, bioengineering, biomedicine, and clinical communities. However, the recent NIH Roadmap demands the formalized development of interdisciplinary teams focused upon defined objectives that require collaborative efforts from multiple fields. It is likely that other countries will adapt a similar strategy.

There are two initial approaches to the long-term successful implementation of strategic planning for research directed to these new pathways of discovery: (i) entice established faculty in different disciplines to collaborate by incentives (funding); (ii) introduce and sustain interdisciplinary training early in the careers of students without compromising depth and rigour in a primary discipline. The NIH Roadmap proposes both approaches and in addition redefines the role of universities by encouraging centers of technical excellence (in addition to intellectual excellence), a role traditionally maintained by government (e.g., NIH, CDC, etc), Institutes of Technology, and contracts to the private sector.

In the US, biofluid mechanics research is positioned to attract (additional) NIH funding by virtue of the interdisciplinary nature of the subject. It will be necessary to overcome infrastructural barriers in US universities that obstruct some aspects of cooperation between faculty in disparate departments and schools which are competing for common resources, even within interdisciplinary departments such as biomedical engineering. The availability of NIH funding targeted to support interdisciplinary collaborations *across* departments (and institutions) will help in this regard as does the establishment of formal interdisciplinary suprdepartmental groupings (institutes, centers) at some universities. Common to all countries is a needed attitudinal change in the traditional cultural differences that exist

between engineering and medical departments, and the sustained education of young people in an interdisciplinary culture that promises a clear career pathway; in the US, biomedical engineering departments and interdisciplinary Centers are perhaps the most appropriate structures to do this. The academic infrastructure varies from country to country; in smaller countries with geographically closely located institutions and smaller budgets, such centers may interfere with other funding priorities. Whatever the country or infrastructure, it is in the interests of Biofluid Mechanics investigators to support such developments.

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